ME 141B: The MEMS Class Introduction to MEMS and MEMS Design

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BioMEMS Case Study: Microdevices for PCR

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Outline

- What is hard about BioMEMS
- BioMEMS success stories
- DNA amplification and PCR
- Two designs
  - A static PCR themocycler
  - A flow-thru design
  - Comparison
- Design evolution of static approach
- Conclusions

BioMEMS

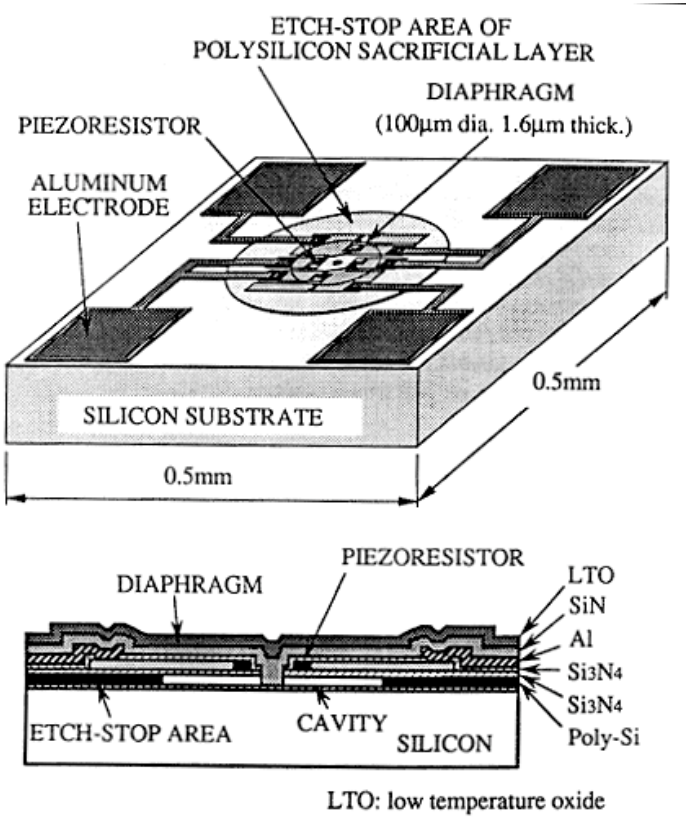
- Applications of microsystems to bioscience
  - Neural probes
  - Capillary electrophoresis
  - Drug delivery
  - Cellular engineering
  - Tissue engineering

What is hard about BioMEMS

- The biological system is poorly defined
  - We fundamentally understand physics
  - We DON'T fundamentally understand biology
  - Thus, only part of system can be truly predicatively designed
- "Intrinsic" biological limitations can dictate system performance
  - Protein-protein interaction kinetics
  - Polymerase error rates
- The materials (and thus processes) are often NOT silicon (and thus harder)
  - We must move away from the most established fabrication technologies

BioMEMS success stories

- Depending on definition, there are very few
- Commercial successes
  - ➢ Blood pressure sensors
    - Low cost “widget” allows devices to be disposable
  - ➢ Affymetrix DNA microarrays
    - Vastly decreases time and cost for analyzing nucleic acids
    - But these are not really bioMEMS



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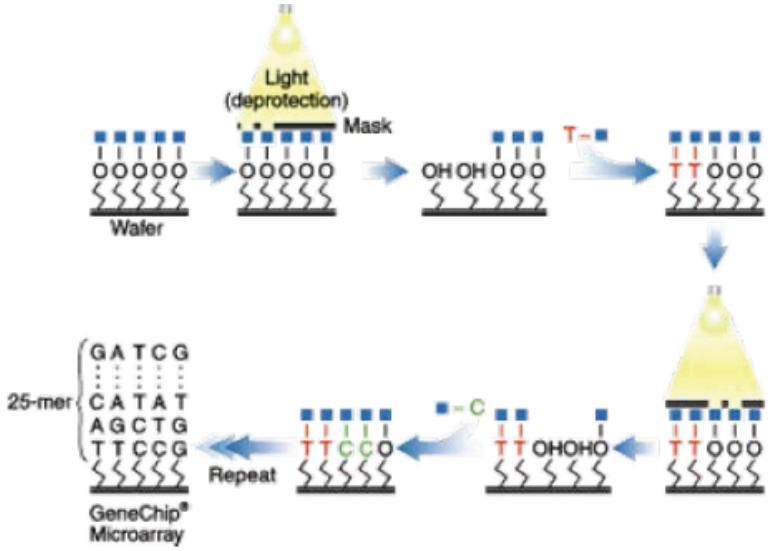
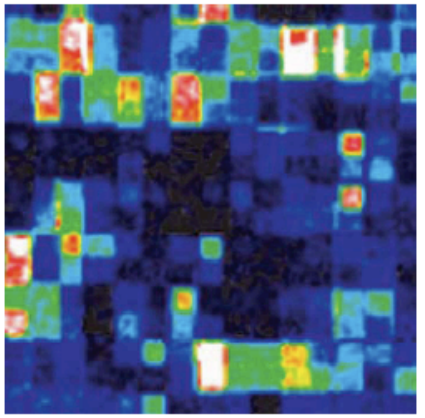
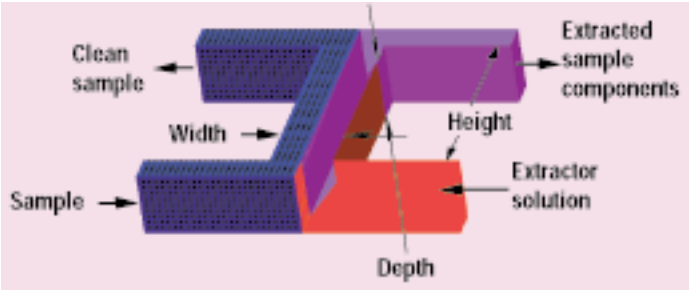


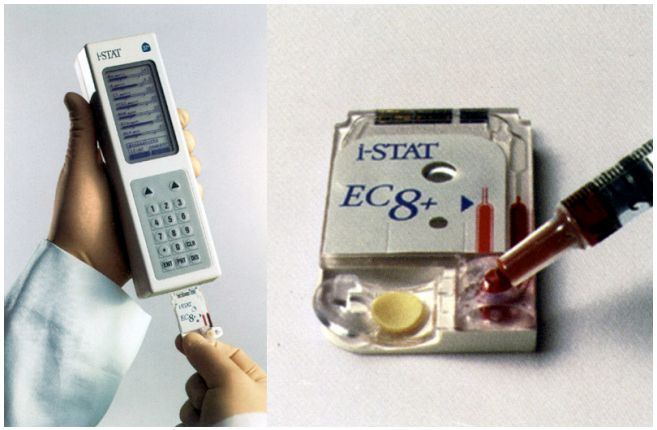
Courtesy of Affymetrix, Inc. Used with permission.



BioMEMS success stories

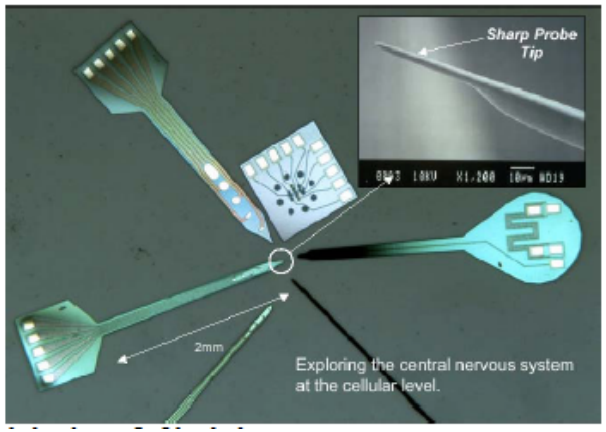
- In the commercial sector, there has been lots of hype
  - Success if uncertain
- Caliper/Aclara
  - Lab-on-a-chip
- I-stat
  - Portable blood analyzer
  - Uses ion-selective electrodes, conductivity, etc. to measure salts, glucose, etc.
  - Introduced ~1997
  - Purchases by Abbott





BioMEMS success stories

- Away from commercial sector and into basic science, more successes arise
- Success can be defined as having impact on the target audience



- Ken Wise's neural probes
  - CMOS + bulk micromachining
  - Puts op-amp right near neural recodring sites → amplifies and buffers weak (~uV) signals
  - These are being used by neuroscientists in actual experiments

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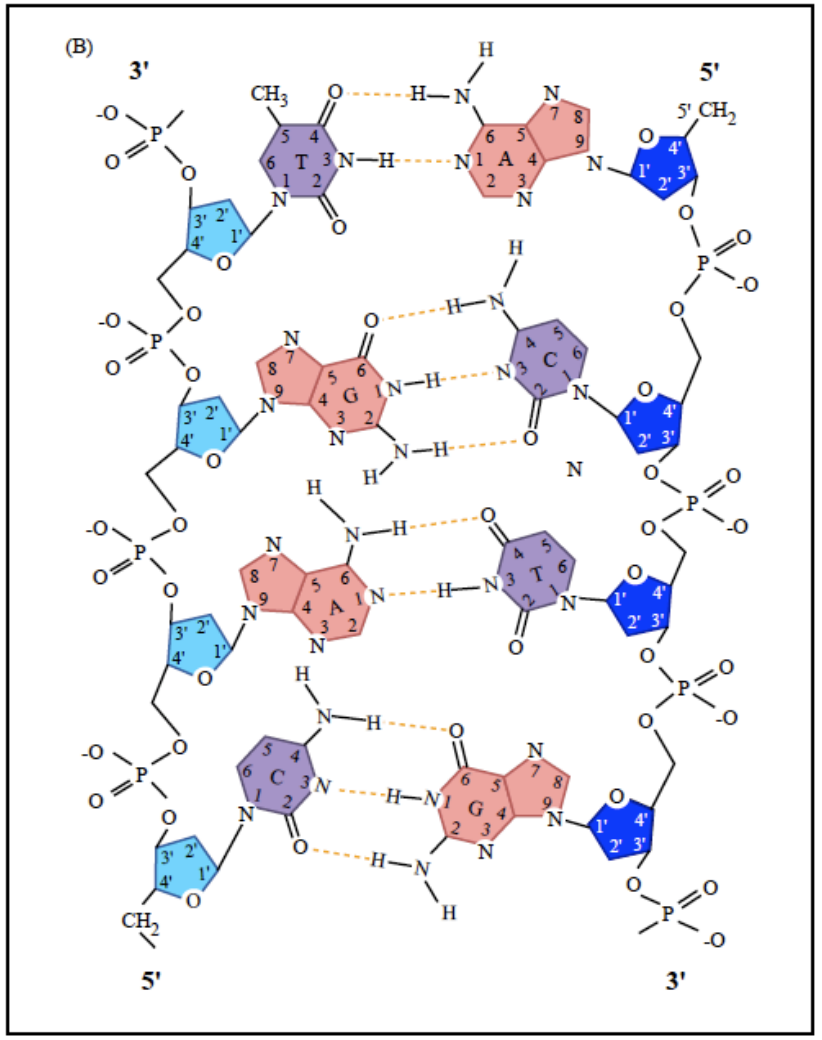
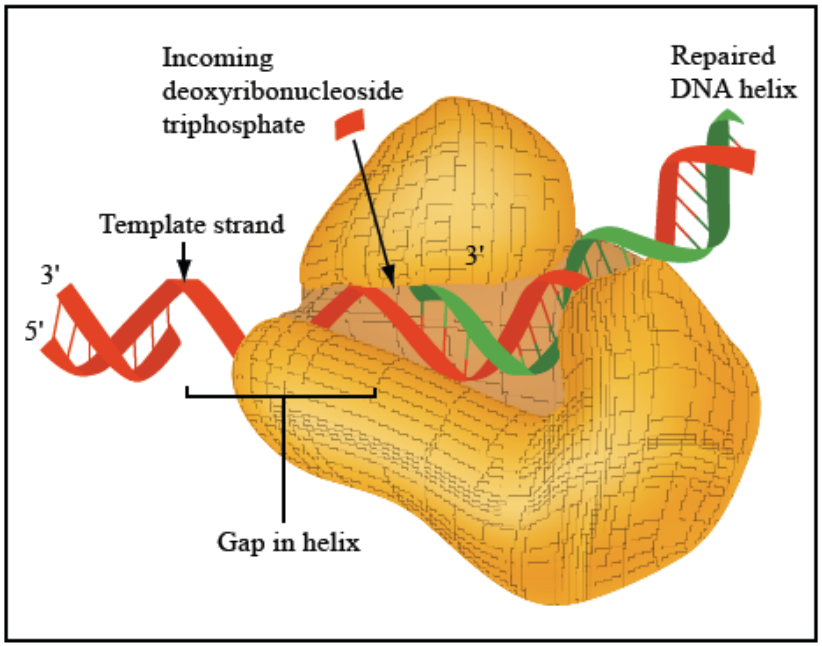
DNA

- DNA → deoxyribosenucleic acid
- DNA contains the genetic information (genotype) that determines phenotype (i.e., you)
- It consists of two antiparallel helical strand
  - Read 5' to 3'
  - A sugar-phosphate backbone
  - Specific bases (A,C,T,G) that contain genetic code
  - This code determined the sequence of amino acids in proteins

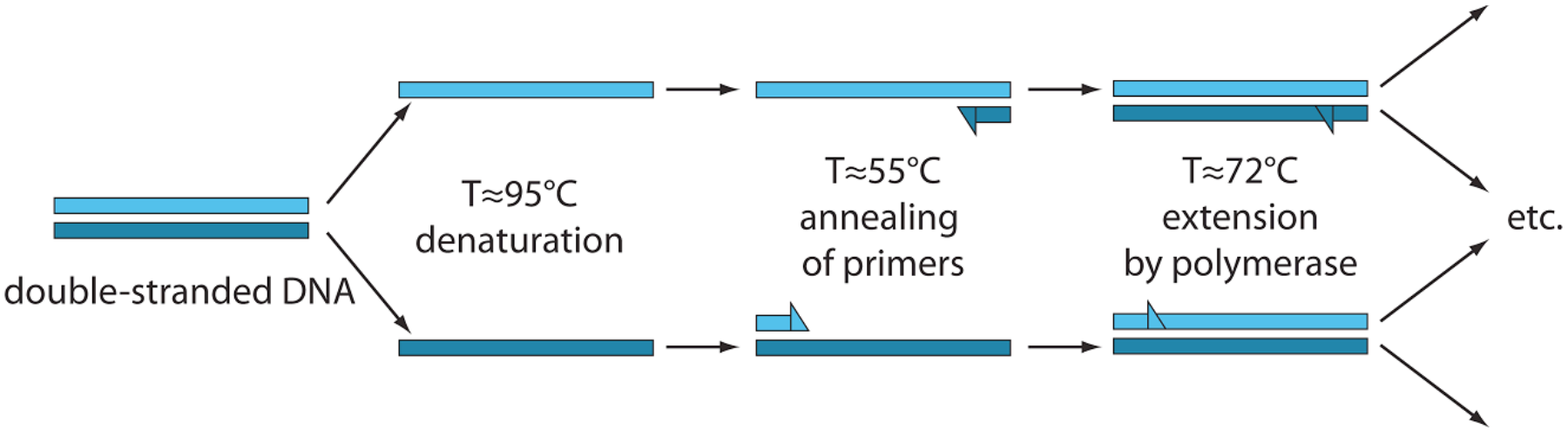


DNA amplification

- The bases pair specifically
  - A with T
  - C with G
- Specific enzymes (DNA polymerases) can add complementary nucleotides to an exisiting template + primer
  - This is done in vivo in DNA replication
- Was capitalized in vitro in polymerase chain reaction
  - Invented in 1985, Nobel Prize in 1993

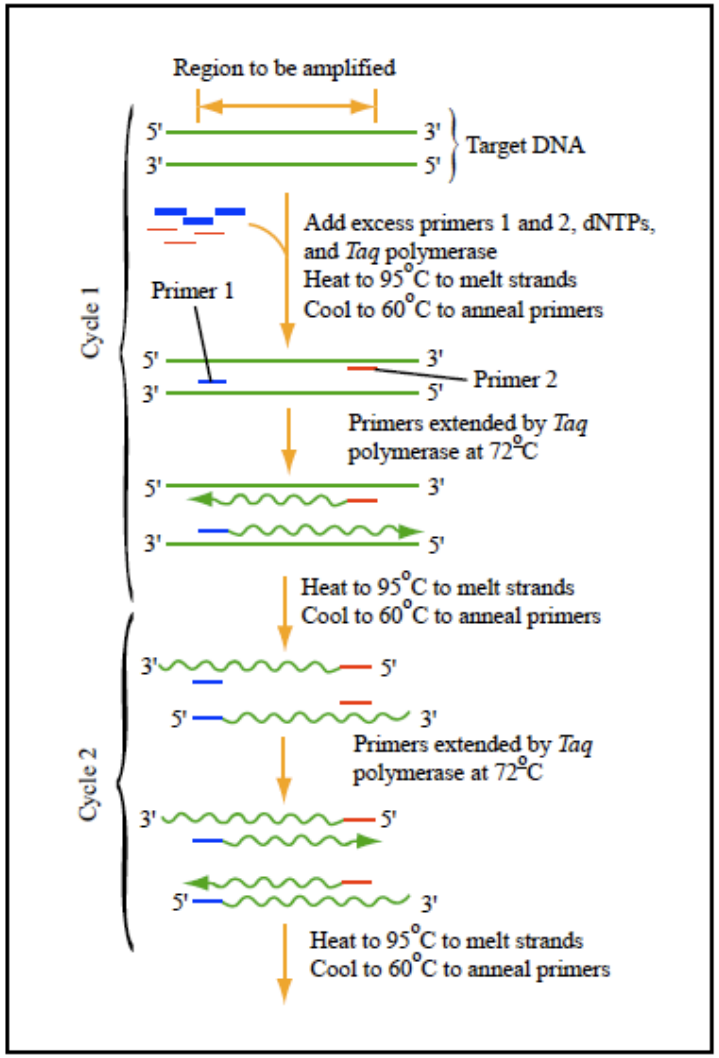


PCR Intro

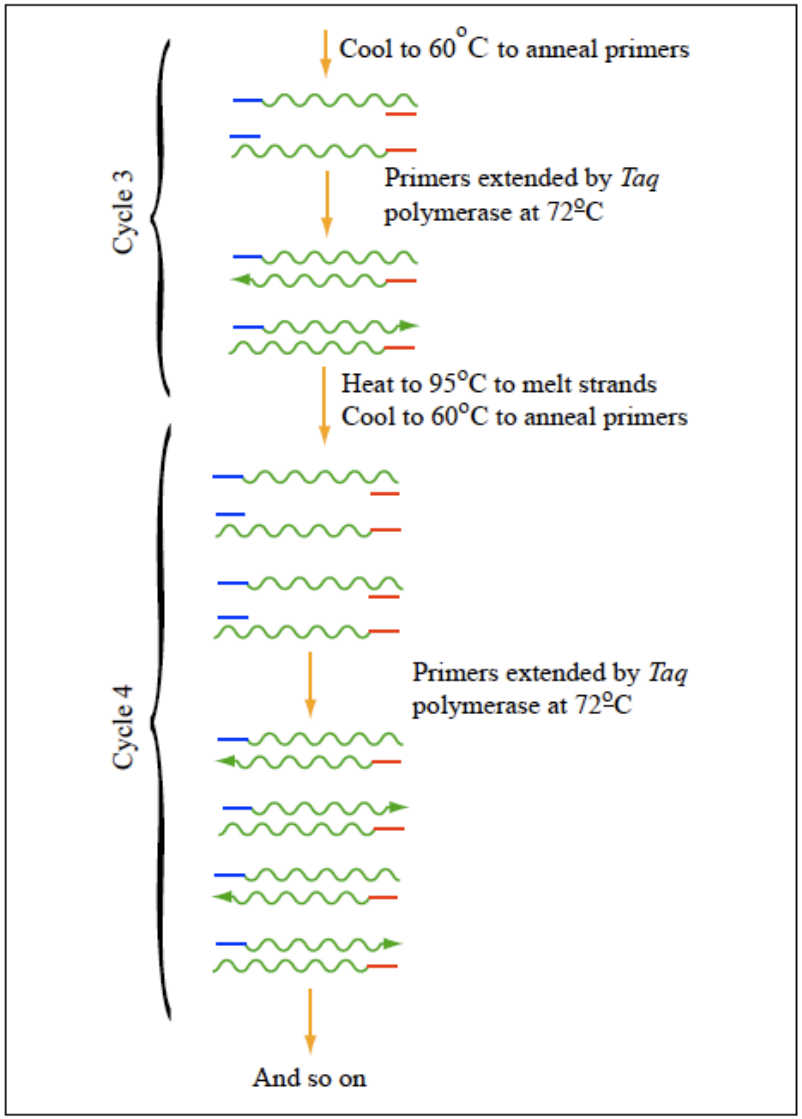

double-stranded DNA
T≈95°C
denaturation
T≈55°C
annealing
of primers
T≈72°C
extension
by polymerase
etc.

Polymerase Chain Reactions (PCR)

- Specifically amplify DNA starting from 1 double-stranded copy



Polymerase Chain Reactions (PCR)

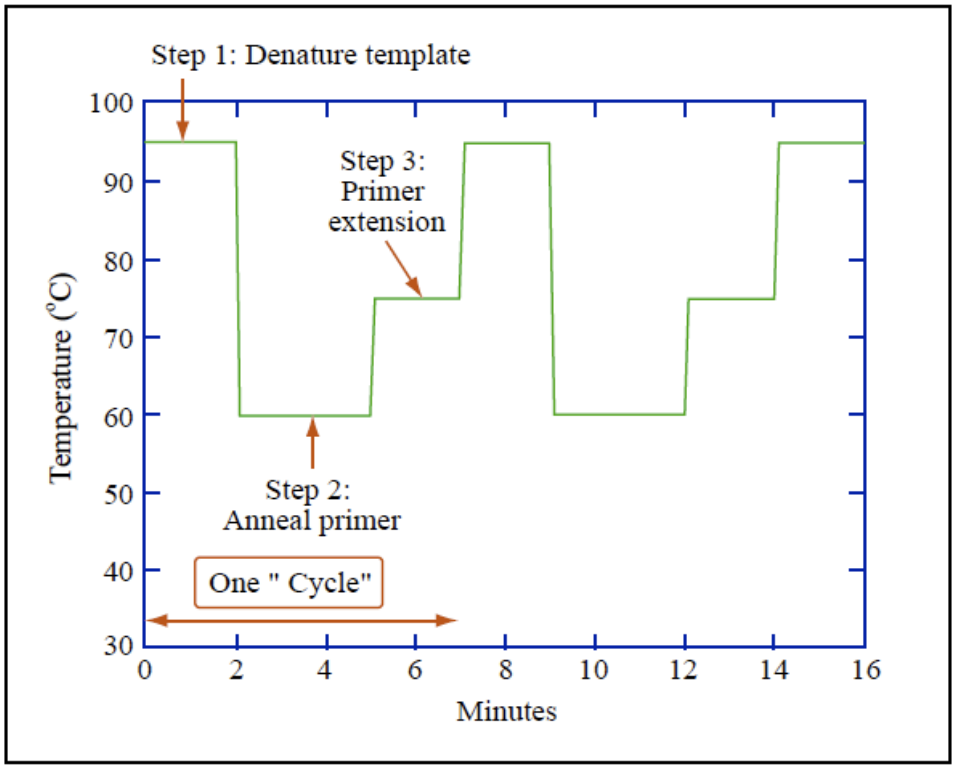


PCR

- Key technological improvement was use of polymerase that could withstand high temperatures
  - Isolated from Thermus aquaticus (Taq)
  - Don't have to add new polymerase at each step
- The device is a simple thermocycler
- Allows amplification and detection of small quantities of DNA

PCR cycles

- *Taq* extension rate ~60nt/ sec
- PCR products are typically a few hundred bases
  - Need ~5 sec for extension
  - Plus time for diffusion
- Typical protocols
  - ~25-35 cycles at 1-3min/ cyce
  - ~30 cycles → 75 minutes



PCR

- Cycle time is dominated by ramp times due to thermal inertia
  - Usually much longer than kinetically needed
- Transient and steady-state temperature uniformity limits cycle time & specificity

Property	Spec
Temp range	5-105 ºC
Set-point accuracy	±0.25 ºC
Temperature uniformity	±0.4 ºC within 30 sec
Heating/cooling rate	~ 3 ºC/sec
Sample volume	50 µl
Number of samples	96
Power required	850 W

BioRad DNA Engine

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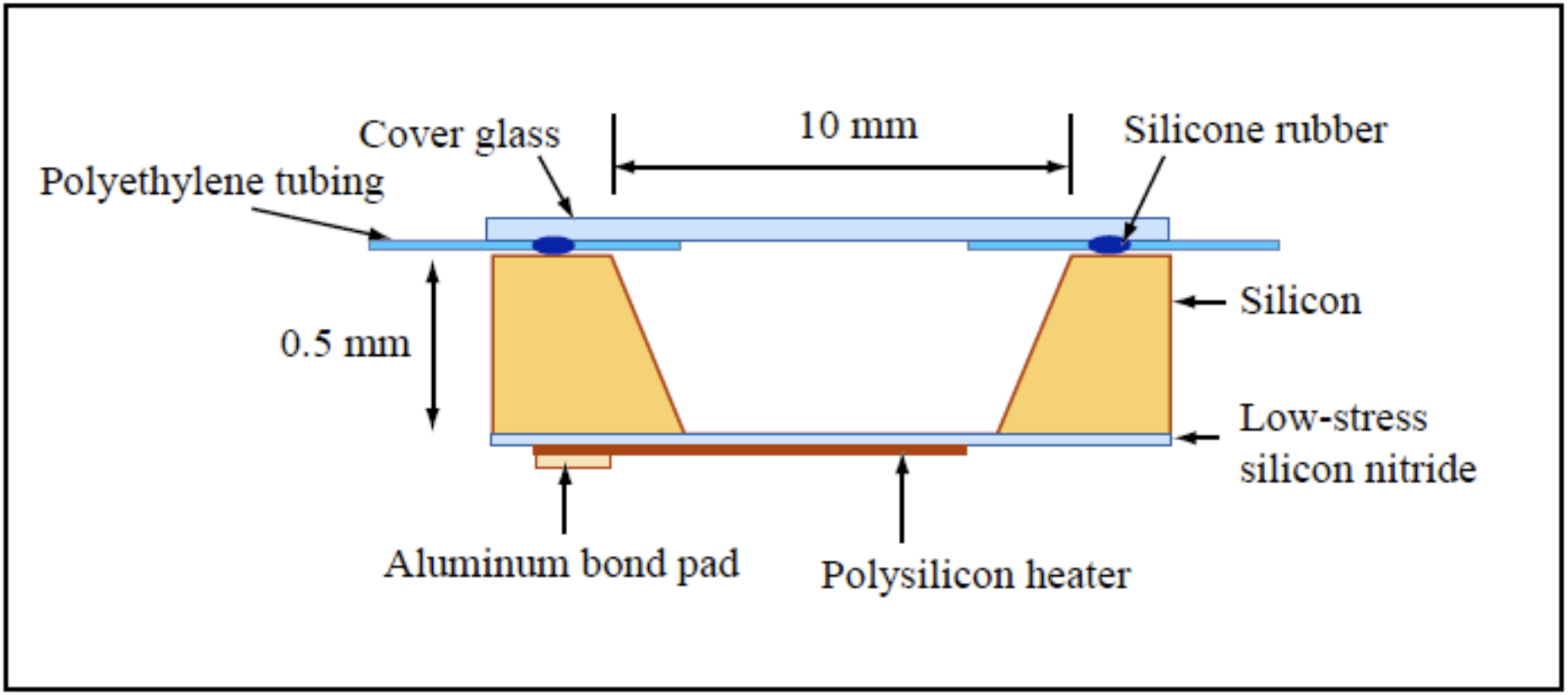
Two approaches to miniaturization

- Decrease size of chamber
  - Vary temperature in time
- Use a flow-thru approach
  - Vary temperature in space (and therefore time)
- In both cases, the device is a thermal MEMS device and the key is to reduce thermal response time

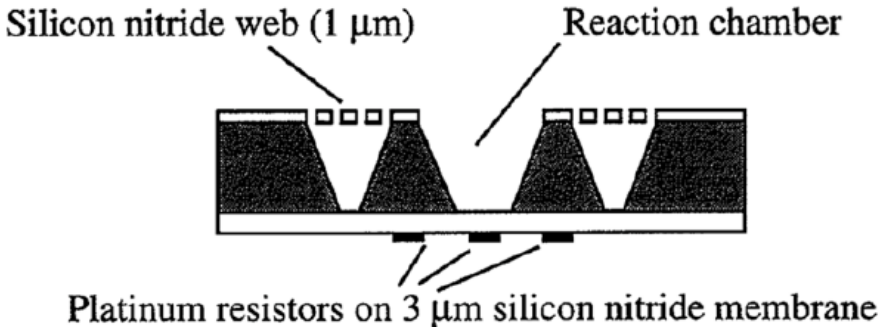
Batch PCR

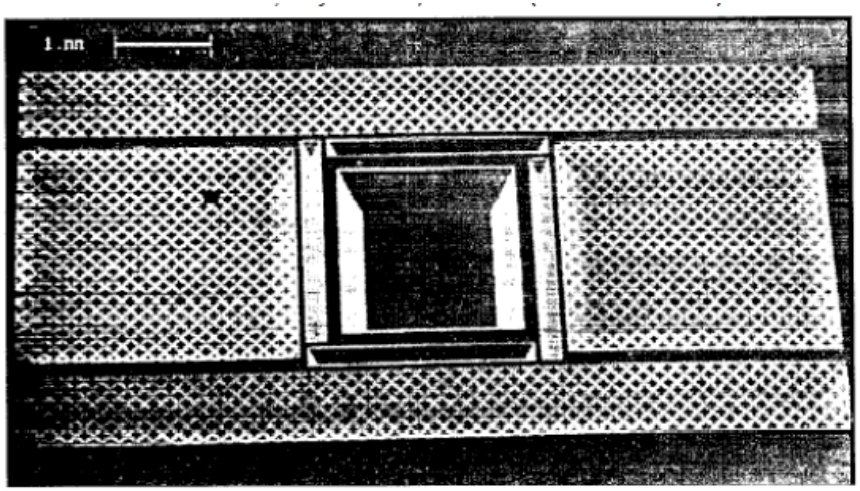
- First reported by Northrup et al. in 1993
  - Essentially a miniaturized thermal cycler

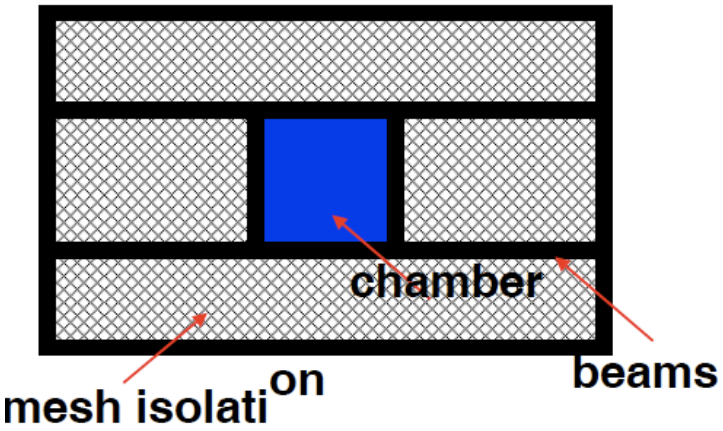


Batch PCR

- Daniel et al. improved thermal isolation

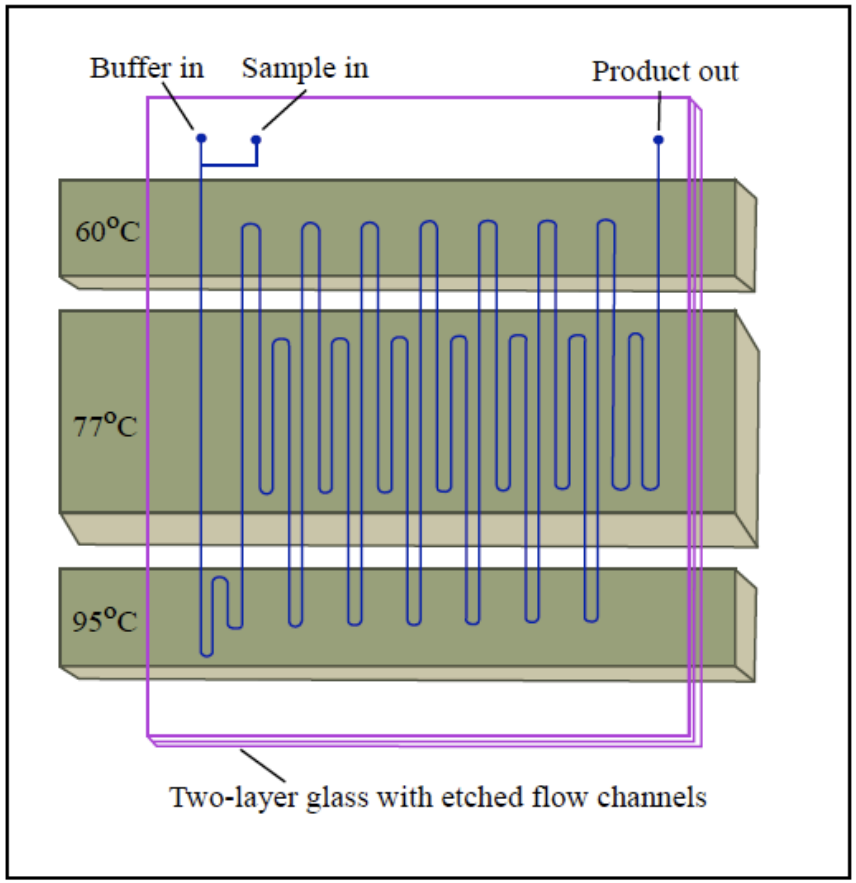


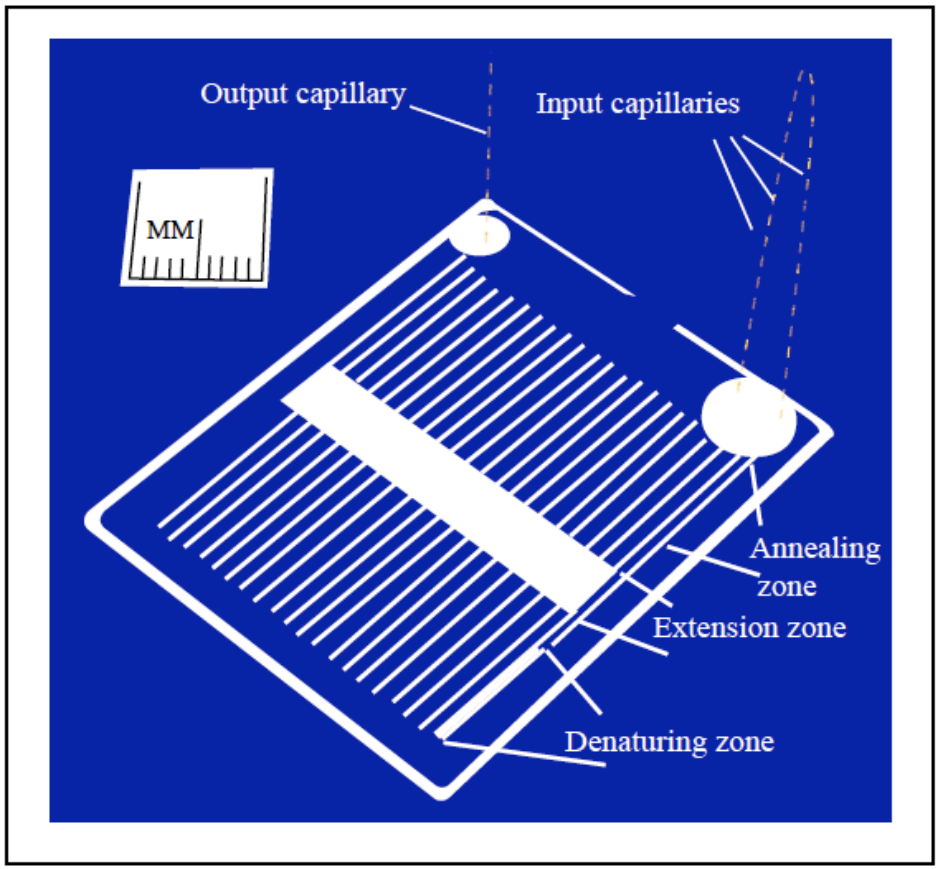




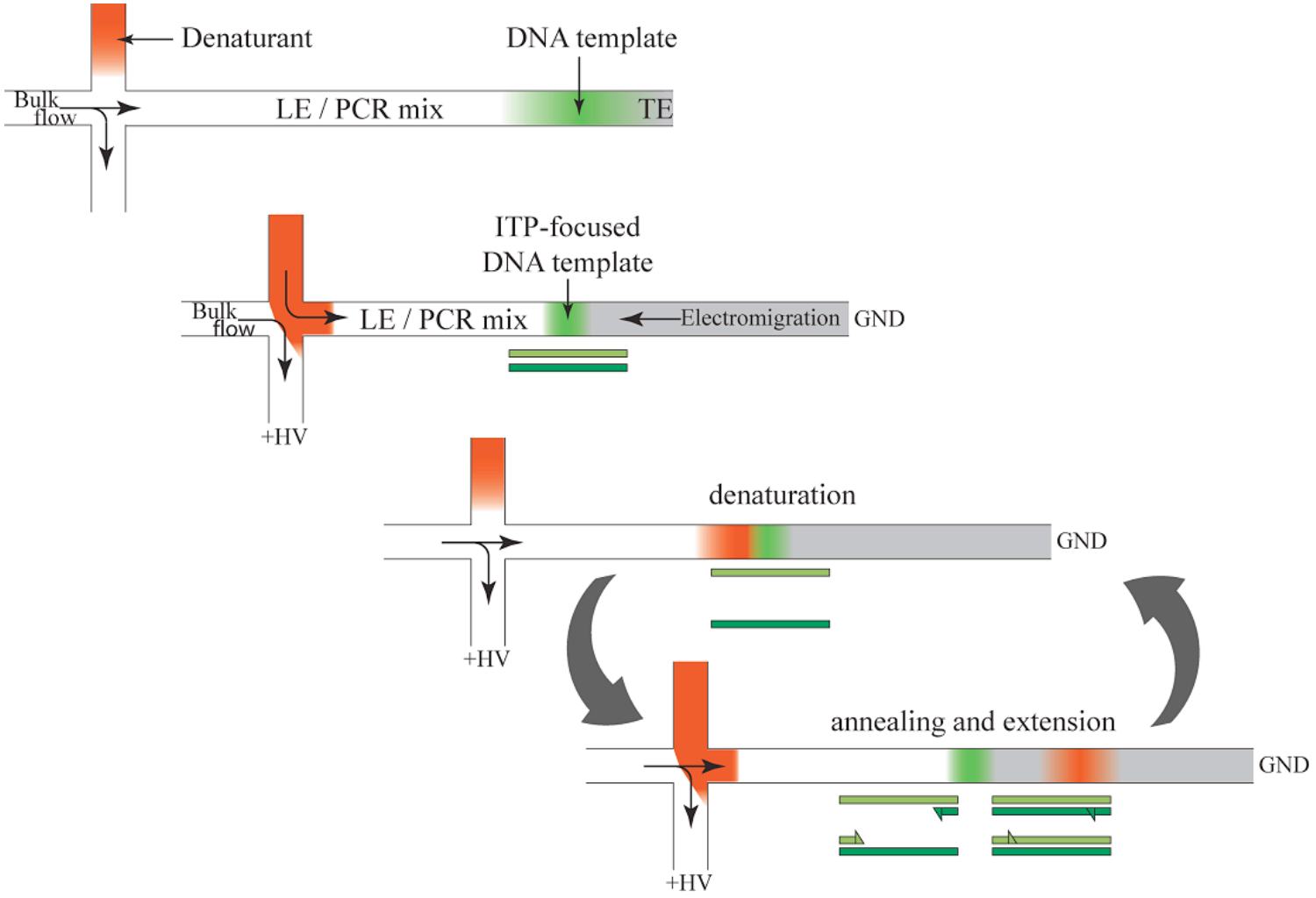
Continuous flow PCR

- Developed by Kopp et al. in 1998

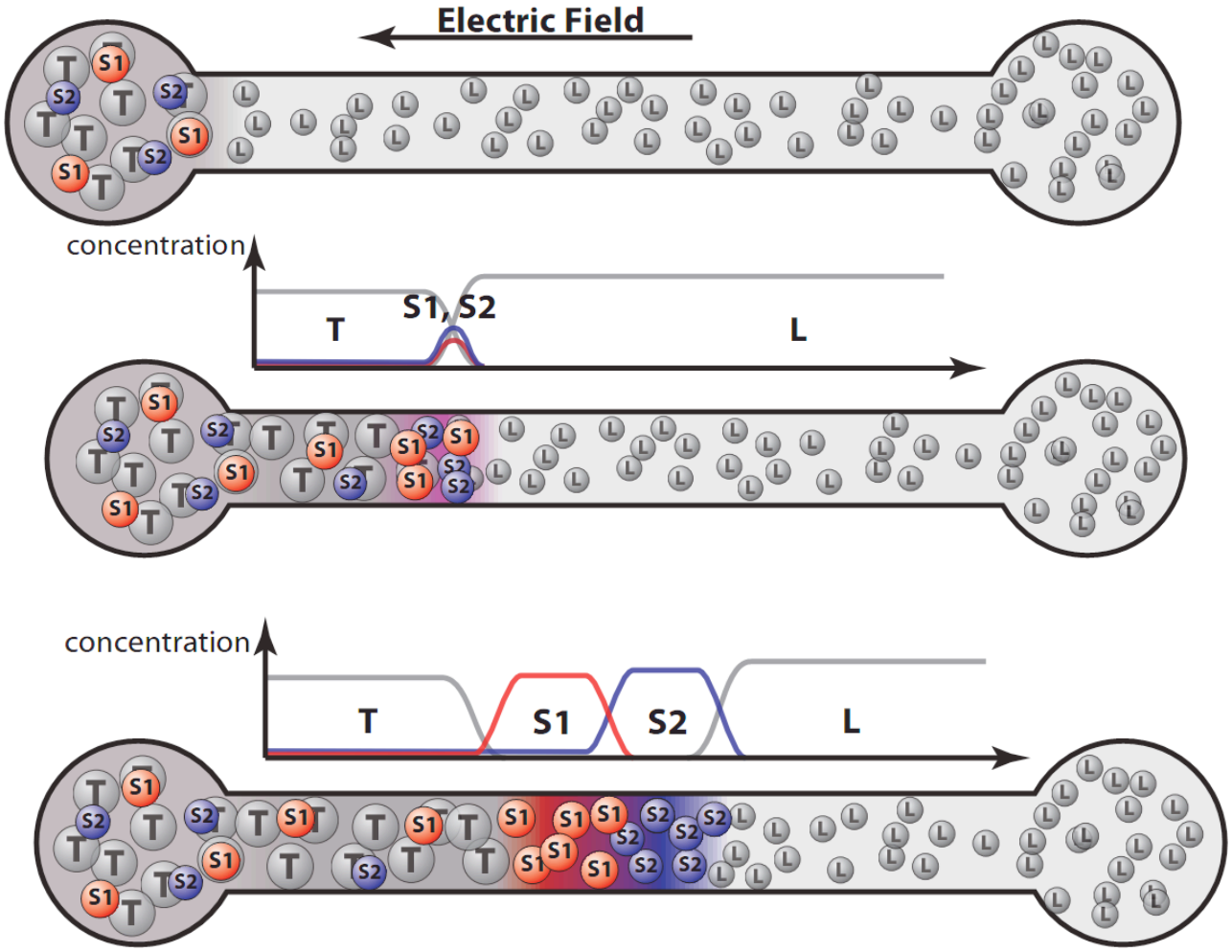




Microfluidic PCR

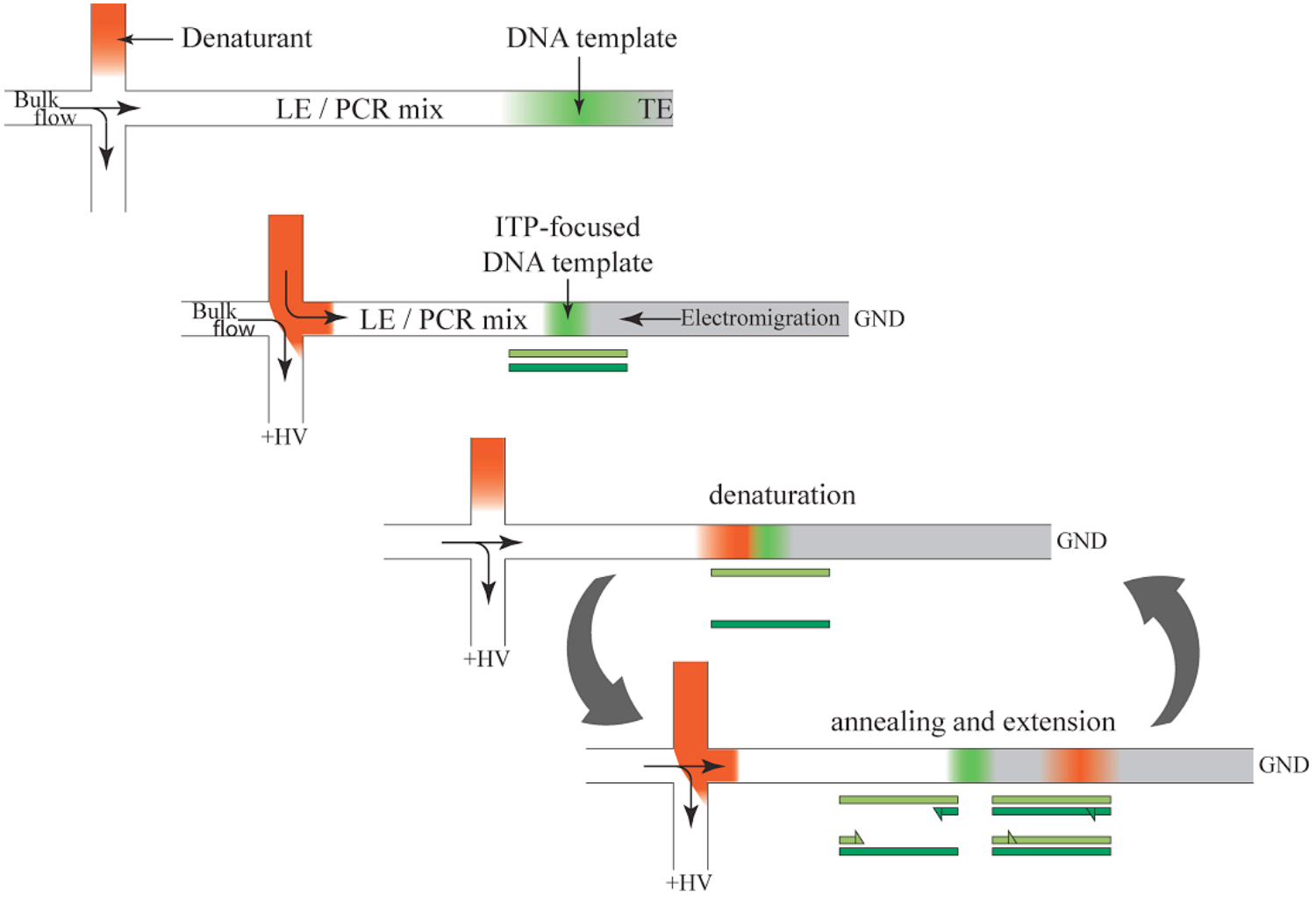


What is ITP?


Electric Field
concentration
T
S1, S2
L
concentration
T
S1
S2
L

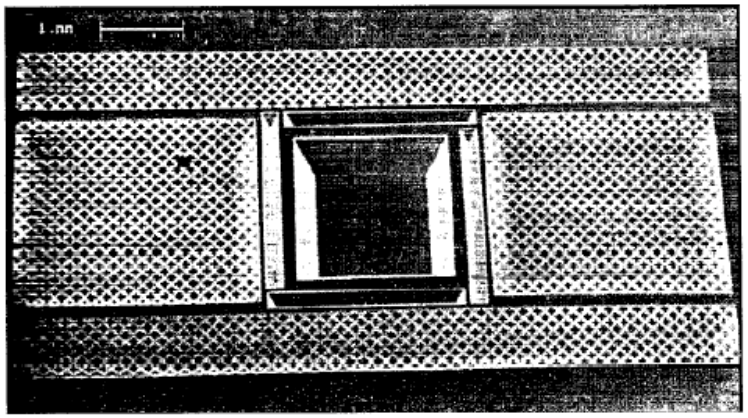

50 μm
TE ions
Sample ions
LE ions

Microfluidic PCR



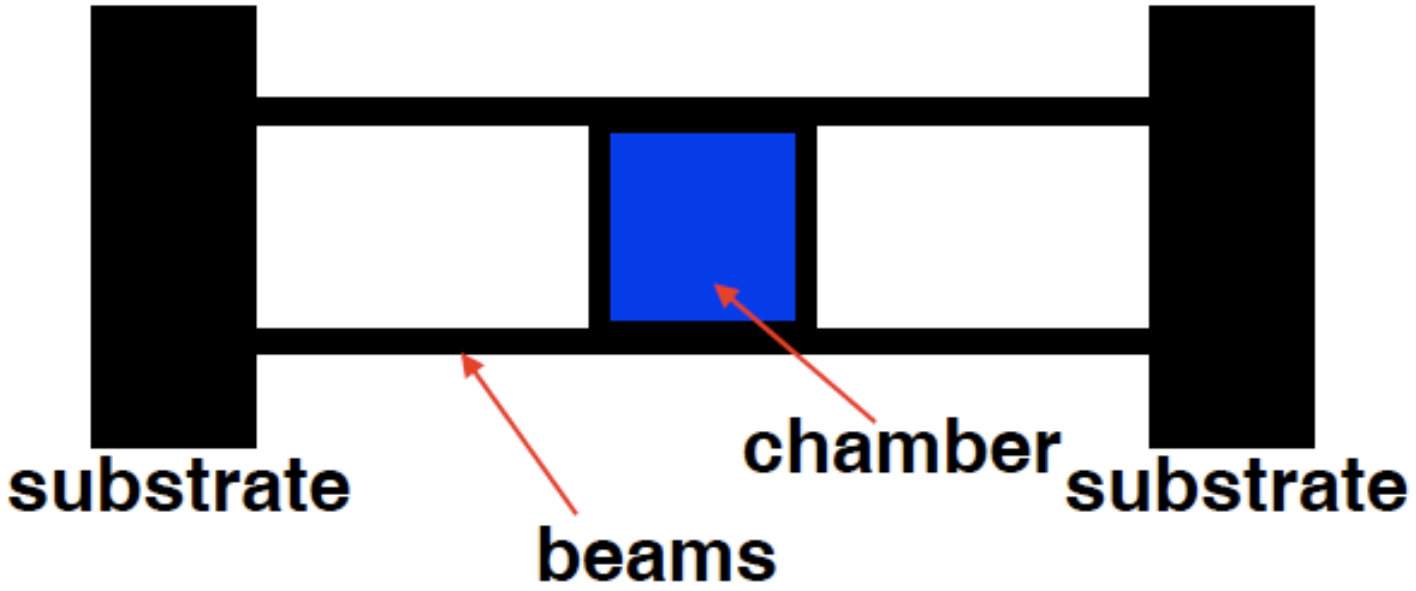
Batch PCR

- Daniel reactor
  - SiN mesh structure, undercut with KOH
    - Made hydrophobic to keep water in chamber during loading
  - Platinum heater resistors heat up beams
  - Two temperature sensing resistors
    - One on beams for feedback control
    - One of membrane to sense “liquid” temp
  - Use oil drop on top of liquid to prevent evaporation



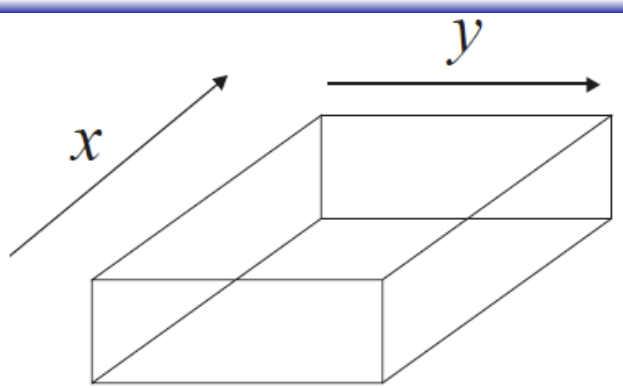
Thermal modeling – batch system

- Three steps
- Model chamber
- Model beams
- Combine the two, with heating at beams



Thermal modeling – batch system

- Chamber model
- Assume rectangular cross-section
- Assume dominant heat loss through beams
  - → 2D heat flow problem
  - ➢ Neglect conduction along top and bottom
  - ➢ Temperature does not vary in z
- Interested in dominant time constant



Eigenfunction expansion solution to heat-flow eqn.

$$T(x,y,t)=\sum_n\sum_m A_{n,m}\cos\left(\frac{n\pi x}{L}\right)\cos\left(\frac{m\pi y}{L}\right)e^{-\alpha_{m,n}t}$$

$$T_1(x,y,t)=A_1\cos\left(\frac{\pi x}{L}\right)\cos\left(\frac{\pi y}{L}\right)e^{-\alpha_1 t}$$

Lowest mode

$$\tau_f=\frac{1}{\alpha_1}=\frac{L^2}{2\pi^2 D}=\frac{L^2\tilde{C}_m\rho_m}{2\pi^2\kappa}$$

Thermal modeling – batch system

- Obtain lumped heat capacity by weighing over model volume
- Extract thermal resistance from time constant
- Thermal resistance same as zeroth-order model suggests

$$C_f = \rho_m \tilde{C}_m \int_{-L/2}^{L/2}\int_{-L/2}^{L/2}\int_{0}^{H} \cos\left(\frac{\pi x}{L}\right)\cos\left(\frac{\pi y}{L}\right) dx\,dy\,dz$$

$$C_f = \rho_m \tilde{C}_m \frac{2L}{\pi}\frac{2L}{\pi} H$$

$$C_f = \frac{4\rho_m \tilde{C}_m L^2 H}{\pi^2}$$

$$\tau_f = R_f C_f \Rightarrow R_f = \frac{1}{8\kappa H}$$

$$R_f = \frac{1}{\kappa}\frac{length \cdot 1/4}{area} = \frac{L/2\,1/4}{\kappa L H} = \frac{1}{8\kappa H}$$

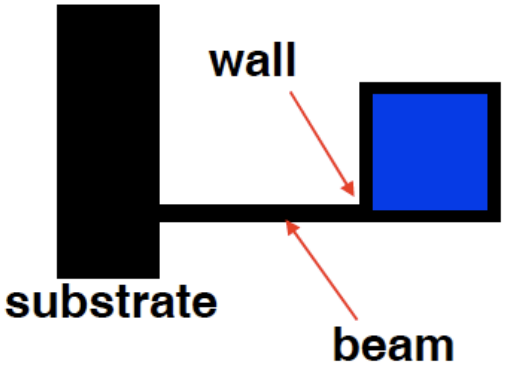
- For L=2 mm, t=1.4 s
- H = 400 um, volume = 2uL

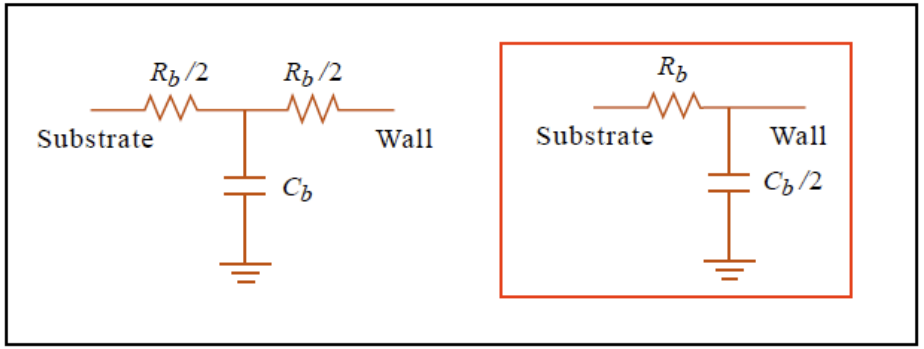
Thermal modeling – batch system

- Lumped elements for beams
  - Include beam capacitance
- Two circuits to model beams
  - Capacitor in center
  - Capacitor at edge
- Both circuits contain same energy in capacitor at steady state
  - Capacitor at edge is simpler

$$R_b = \frac{1}{4}\frac{1}{\kappa}\frac{length}{area}$$

$$C_b = \rho_m \tilde{C}_m volume$$





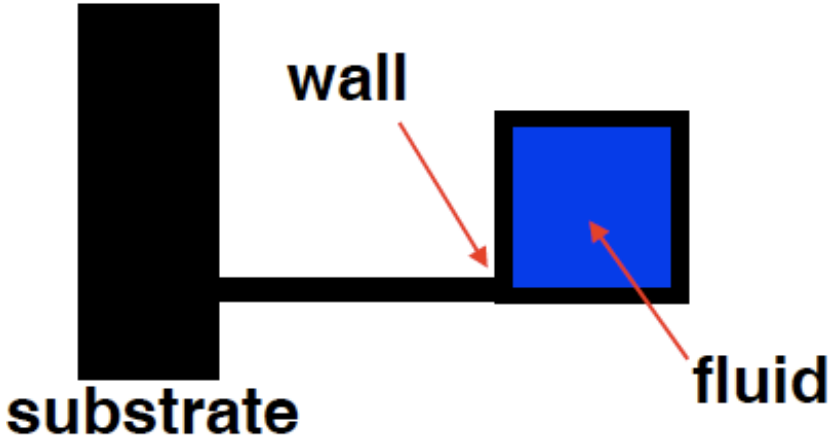
Thermal modeling – batch system

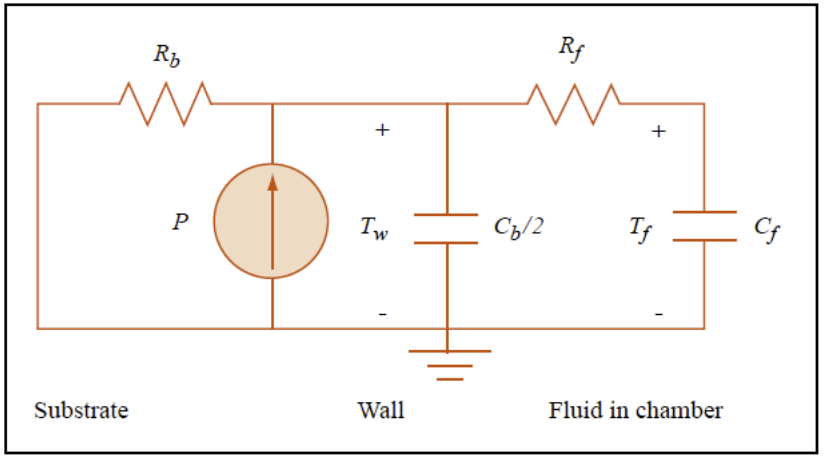
- Lumped circuit model of reactor
- First-order lag between wall and fluid temperature

$$T_f = \frac{1}{1+\tau_f s} T_w$$

$$\tau_f = \frac{L^2}{2\pi^2 D}$$

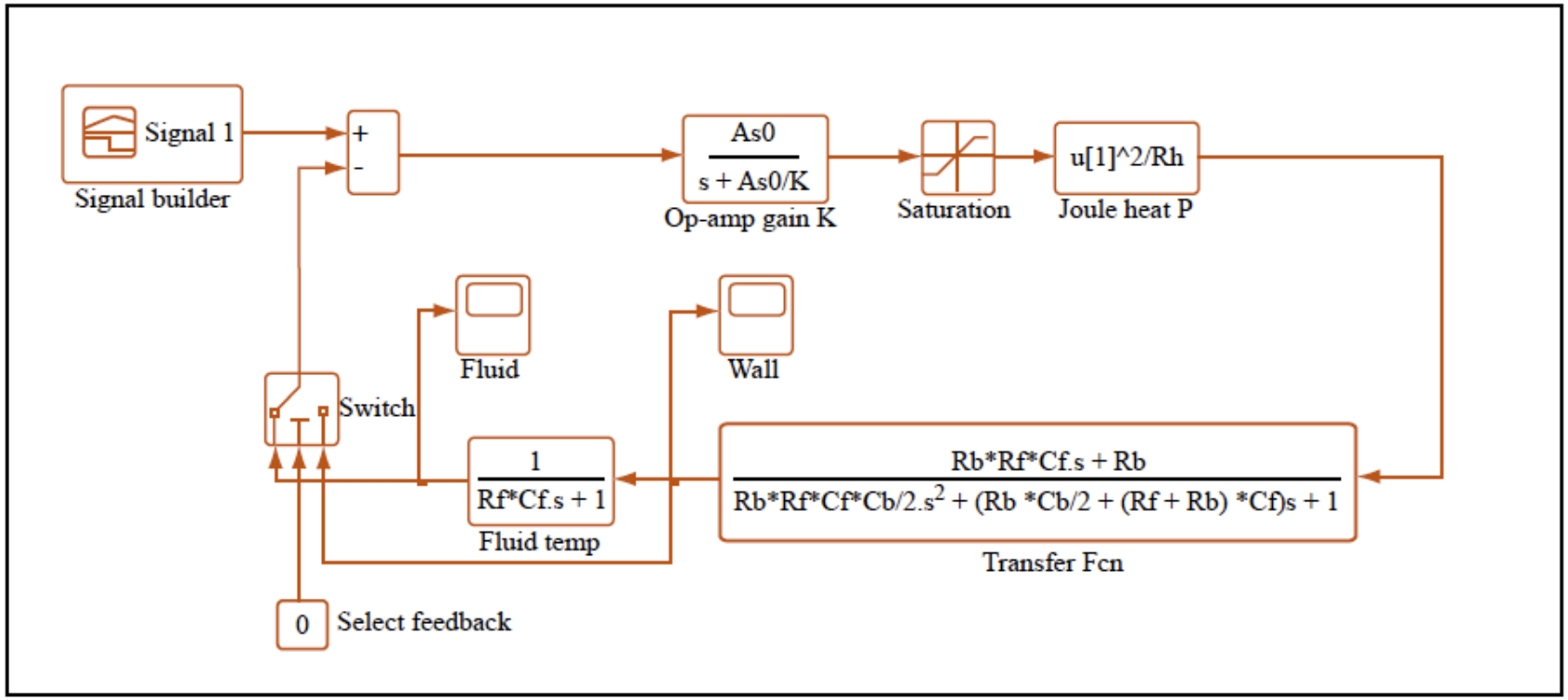
- Making L smaller reduces lag





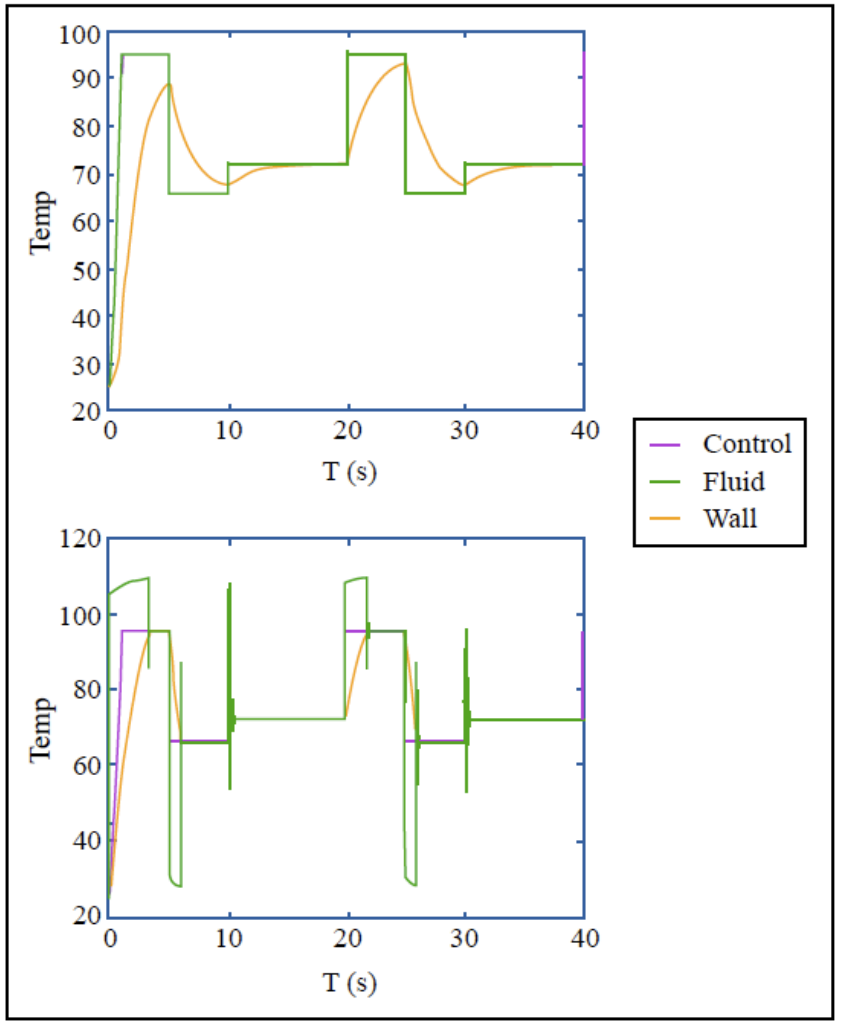
Thermal modeling – batch system

- Simulink proportional control circuit
- Saturation needed for maximum +/- voltage swing
  - Set to 0 to 15 V



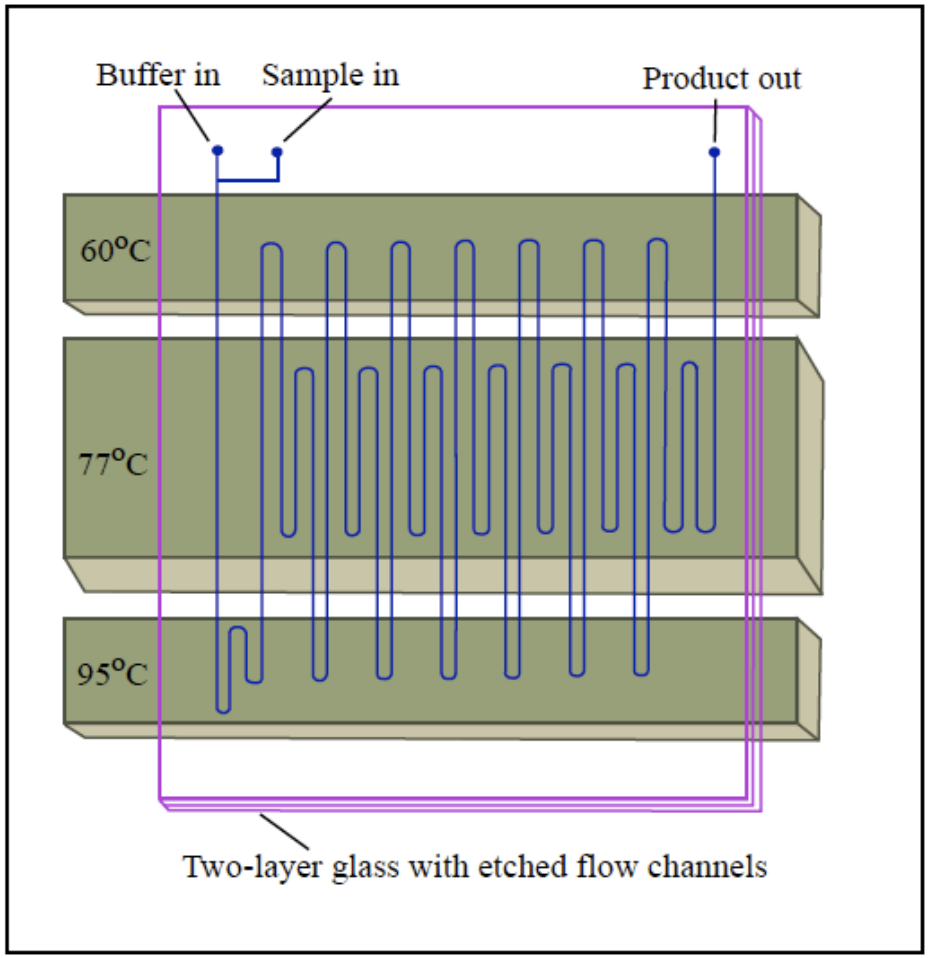
Simulation response

- Wall temperature can be controlled very quickly
- Wall to fluid hear transfer limits performance
- Sensing fluid temperature marginally reduces response times
  - ➢ But creates high-temperature regions at chamber wall



Continuous Flow device

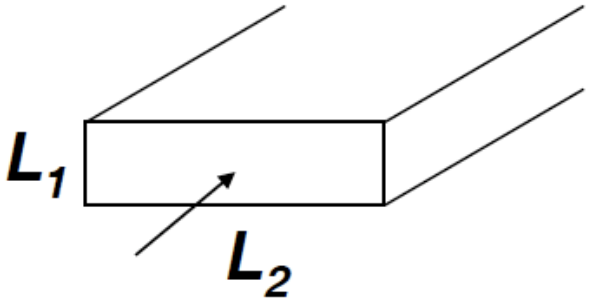
- Systems partitioning: put heaters off-chip
- Etch channels in glass, bond glass cover



Thermal model of continuous flow device

- Wall-to-fluid time constant is same as in batch device
- L_1=40 μm, L_2=90 μm
- D=1.4x10^{-7} m^2/s
- τ_f= 1.2 ms
- 1000× faster than batch device!

$$\tau_f = \frac{L_1 L_2}{2\pi^2 D}$$



- Entrance length for thermal equilibration

$$L_e \approx 3 v_f \tau_f$$

- Average flow velocity

$$v_f = \frac{Q_f}{area} = 20 \text{ mm/s}$$

$$L_e \approx 60 \ \mu\text{m}$$

This is much smaller than zone lengths

- Thermal Pe number is ~10^{-3}

Continuous-flow device

- What about Taylor dispersion
- Pressure-driven may cause multiple camples to coalesce
- Hydrodynamic radius of 1 kb DNA ~ 50nm
- Dispersivity is dominated by convection
  - Samples will spread out a lot, limited usefulness for multiple samples

$$D = \frac{k_B T}{6\pi\eta R}$$

$$Pe = \frac{LU}{D} = \frac{(40\mu m)(0.02 m/s)}{4.4x10^{-8} cm^2/s} \sim 2x10^5$$

$$K = D\left(1 + \frac{Pe^2}{210}\right) f\left(\frac{L_1}{L_2}\right)$$

$$\frac{L_1}{L_2} \sim 0.4 \rightarrow f\left(\frac{L_1}{L_2}\right) = 4$$

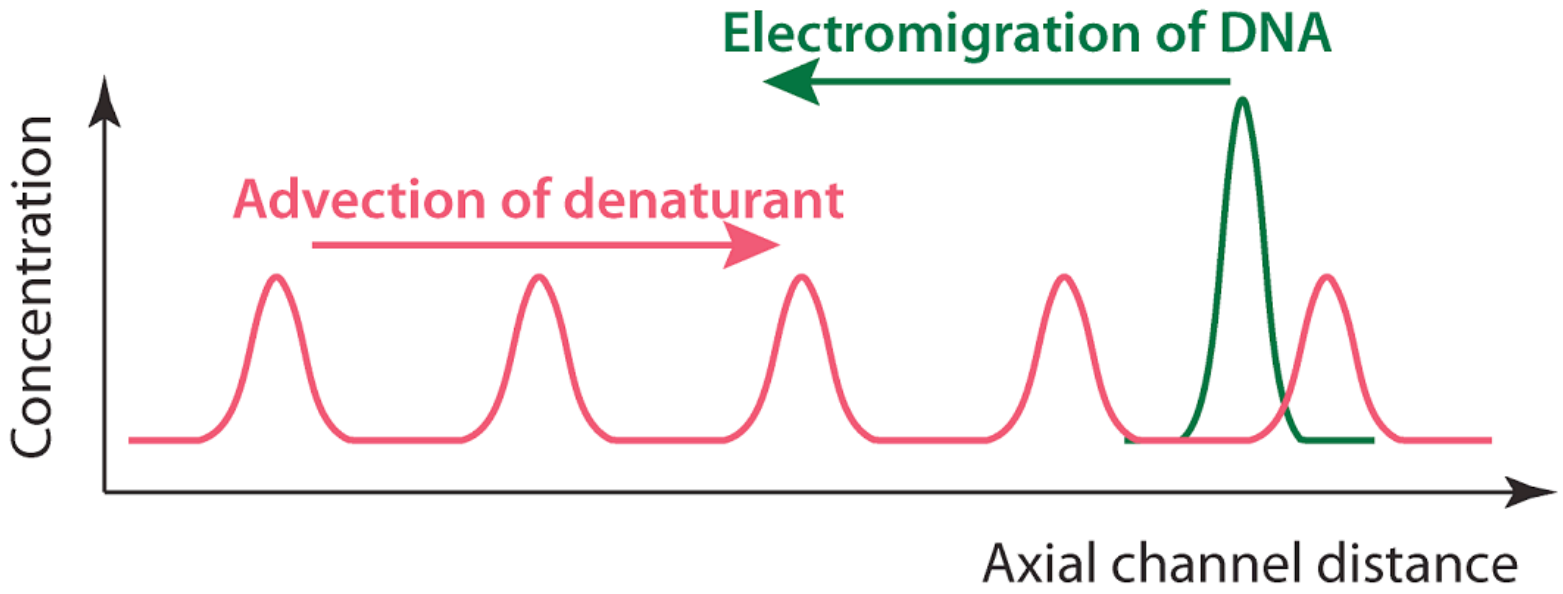
$$K \sim 8x10^8 \cdot D \sim 35\, cm^2/s$$

Thermal Lessons

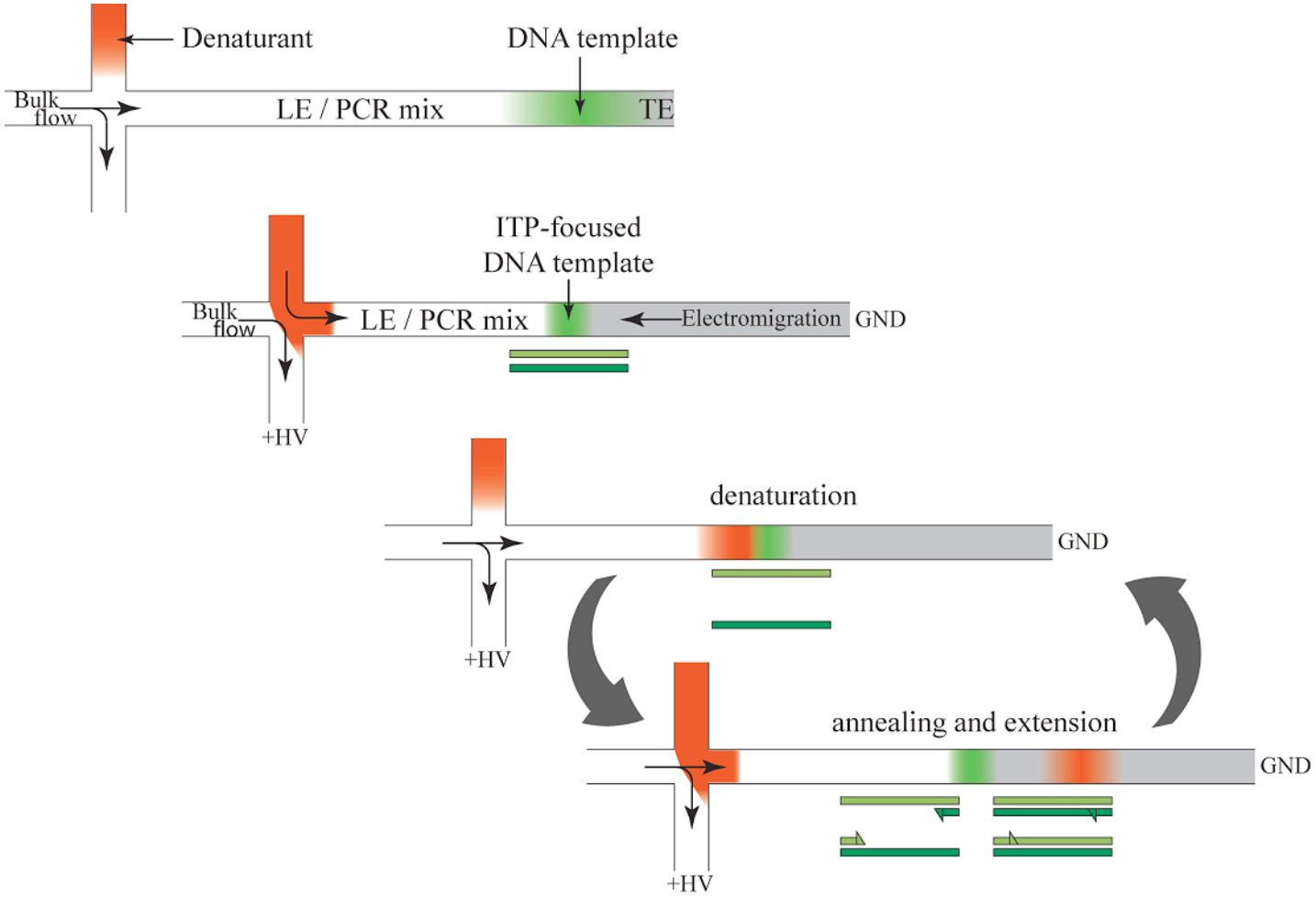
- Wall temperature in most microsystems can be quickly controlled
- Limiting step is wall-to-fluid heat transfer
- Solution is to minimize fluid characteristic length for heat diffusion

Microfluidic PCR

- Temperature is held constant in space and time
- Focus particles using ITP
- Drive DNA sample with ITP through denaturant concentration zones
- High/Low concentrations since denaturant in neutral

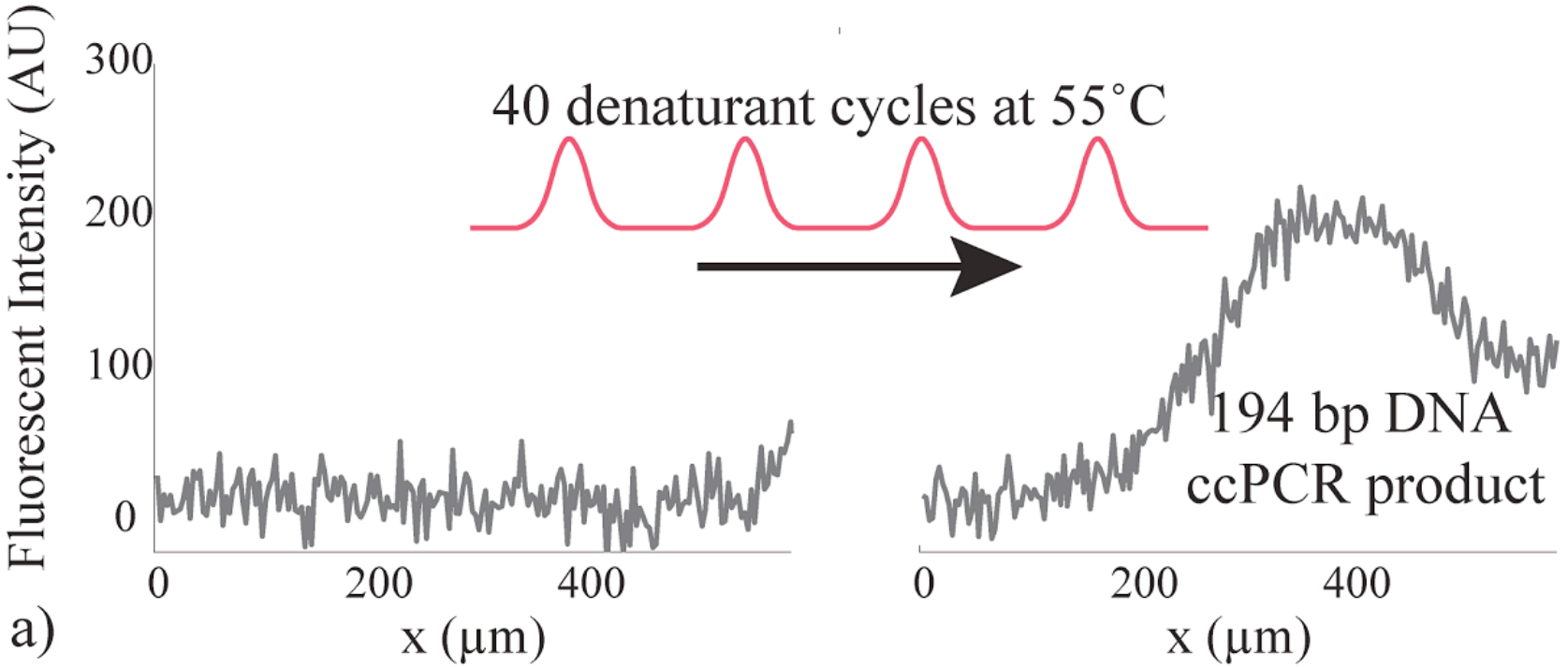


Microfluidic PCR



Microfluidic PCR

- Can use thermostable polymerase
- Reduces power consumption

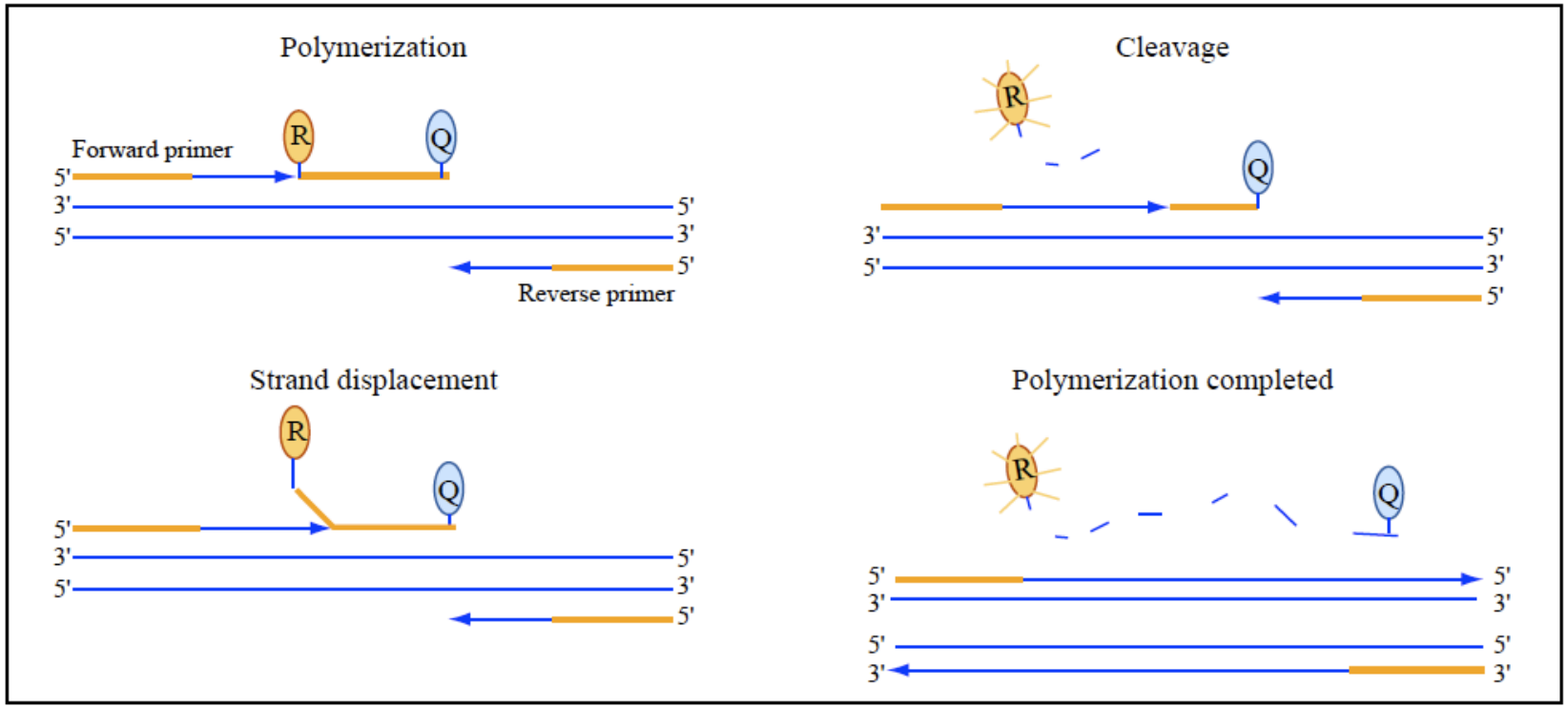


Detecting PCR products

- Speeding up amplification is only half the battle
- DNA is not normally visible
- In conventional PCR, detect products by separating stained DNA using electrophoresis in gel sieving matrix
  - ➢ This can take 0.5-2 hours

Detecting PCR Products

- Newer techniques allow real-time detection
  - "real-time PCR"
- Integrate illumination/detection optics, thermal cycler, and chemistry



Comparison of thermo

Continuous flow	Batch
Faster thermal response	Slower
No temp overshoot	Depends on control system
Static protocol	Can change protocol easily
Taylor dispersion effects, and sample carryover	Sample carryover only
Optical detection more complicated	Simpler optical detection

Materials issues

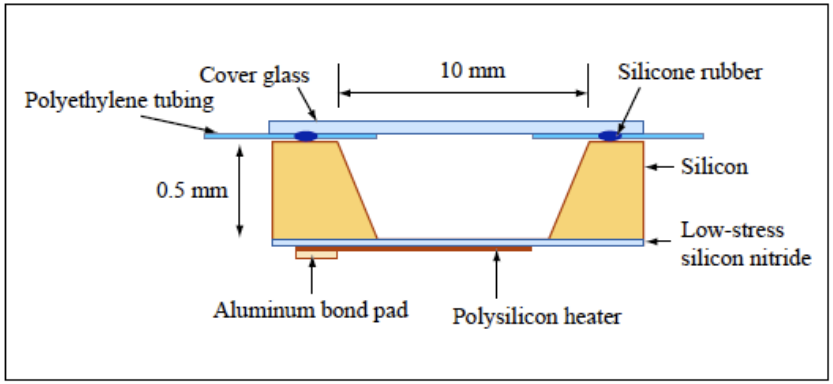
- Reactor surface must be compatible with PCR reagents
  - DNA, nucleoside triphosphates, poymerase, buffers
- Decreasing length scale and increasing SA/V hurts here!
  - More molecules start to interact with surface
- Bare Si or SiN inhibits PCR
  - Probably due to denaturing of polymerase at surface
  - Silanizing or depositing/growing SiO_2 helps
  - Add carrier protein (e.g., BSA) to “block” surface
- Kopp uses glass, silanization, surfactant, and buffer!
- Northrup used deposited SiO_2 plus BSA

Outline

- What is hard about BioMEMS
- BioMEMS success stories
- DNA amplification and PCR
- Two designs
  - A static PCR themocycler
  - A flow-thru design
  - Comparison
- Design evolution of static approach
- Conclusions

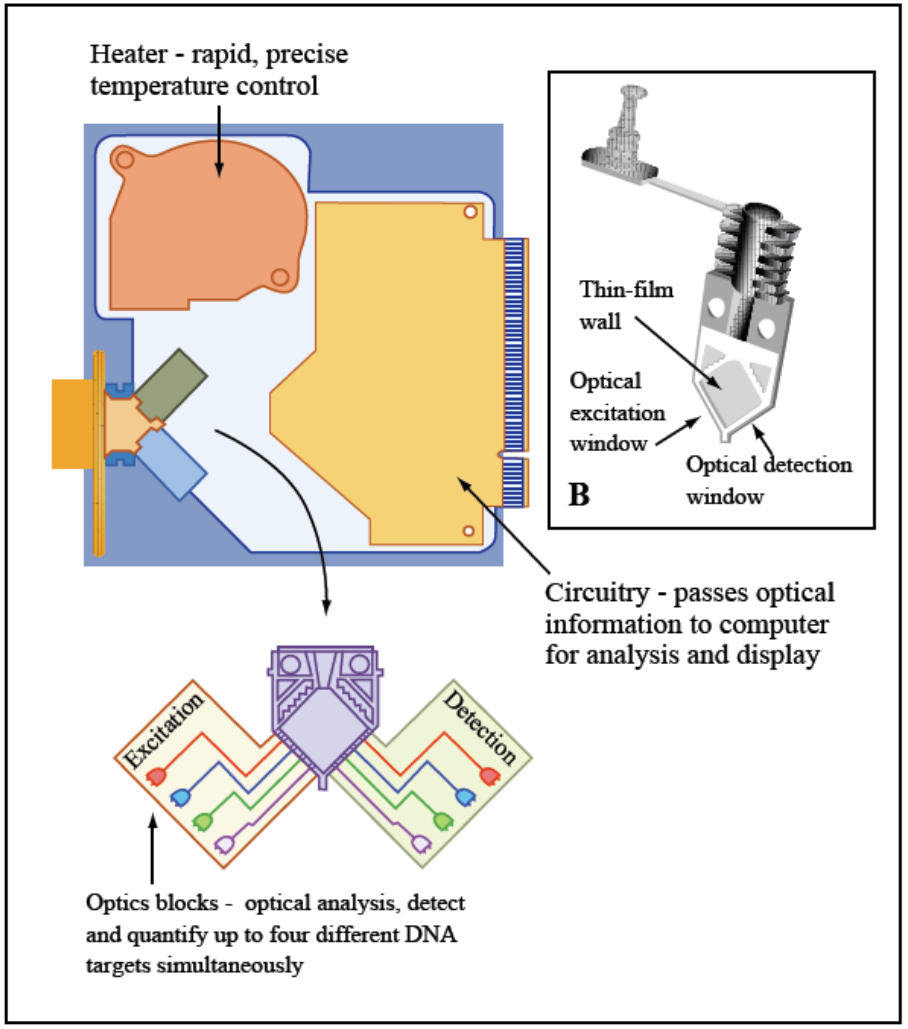
Evolution of chamber device

- Initial device introduces in 1993
- 1995-1996
  - Two heater chambers
  - Improved surface coating
  - Fan for colling
  - Camber volume 20uL
  - 20 sec cycle time
  - Real time PCR coupled to electrophoresis
  - Cepheid formed
- 1998
  - Same two-heater chambers
  - Portable application



Evolution of chamber device

- 2001 to present
  - Abandoned silicon → moved to plastic and NOT microfabricated
  - Tubes are disposable thin-wall 50um plastic that expands upon introduction
  - Tube is flat to decrease thermal reponse
  - ~30 sec cycle time
  - Ceraminc hamber with thin film heater
  - Thermistor temp sensor



Conclusions

- BioMEMS commercial successes are till not here
- Designing the engineered part is often routine
- Interfacing with biology is where it gets hard
- Sometimes the right solution is to NOT microfab